



# Simulating Hearing Loss

## Delft University of Technology

Leo Koop

April 9, 2015

# Outline

## 1 Introductions and Motivation

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The Ear and Cochlea

## 2 Modeling the Cochlea

The General Model

Linear and Non Linear Models

## 3 Simulating Hearing Loss

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The Linear Case; A Sound Filter

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# Simulating Hearing Loss

- Applied Mathematics Department at TU Delft
- Supervisor: Kees Vuik



# Simulating Hearing Loss

- An incas<sup>3</sup> project
- Supervisor: Peter van Hengel



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# Motivation - Hearing Loss, Becoming more Prevalent



Media centre Publications Countries Programmes Governance About WHO

## Media centre

### 1.1 billion people at risk of hearing loss

WHO highlights serious threat posed by exposure to recreational noise

Press release

27 FEBRUARY 2015 | GENEVA - Some 1.1 billion teenagers and young adults are at risk of hearing loss due to the unsafe use of personal audio devices, including smartphones, and exposure to damaging levels of sound at noisy entertainment venues such as nightclubs, bars and sporting events, according to WHO. Hearing loss has potentially devastating consequences for physical and mental health, education and employment.

# Motivation - Uses of a Hearing Loss Simulator

- Education



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- Education
- Hearing loss prevention

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- Education
- Hearing loss prevention
- Simplifying hearing aid development and testing

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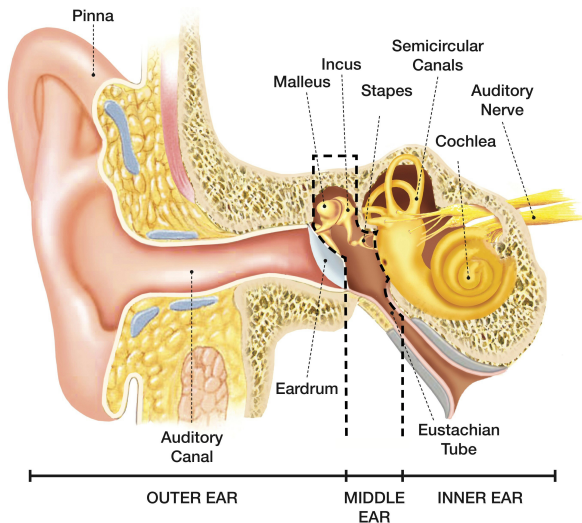
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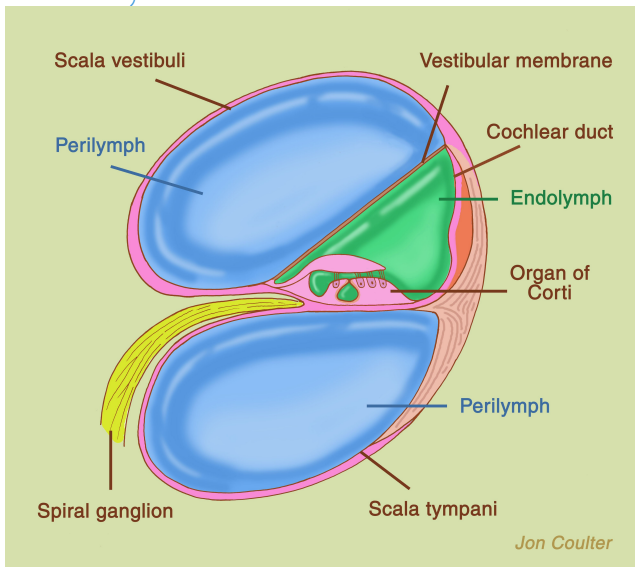
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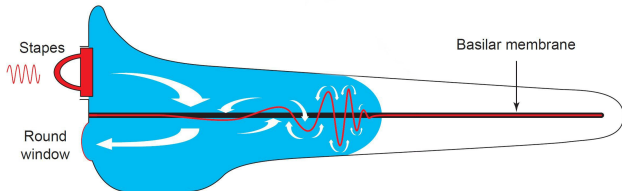
# The Ear



# The Cochlea, a Cross Section



# The Cochlea



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# Modeling the Cochlea

## The Main Equation

$$\frac{\partial^2 p}{\partial x^2}(x, t) - \frac{2\rho\partial^2 y}{h\partial t^2}(x, t) = 0, \quad 0 \leq x \leq L, \quad t \geq 0 \quad (1)$$



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- $p(x, t)$ : Pressure on the cochlear partition

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- $y(x, t)$ : The excitation of the oscillator
- $p(x, t)$ : Pressure on the cochlear partition
- $\rho$ : Density of the cochlear fluid
- $h$ : Height of the scala
- $L$ : Length of the cochlea
- $t$ : Time

# Modeling the Cochlea

The pressure term

$$p(x, t) = m\ddot{y}(x, t) + d(x)\dot{y}(x, t) + s(x)y(x, t) \quad (2)$$

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## The pressure term

$$p(x, t) = m\ddot{y}(x, t) + d(x)\dot{y}(x, t) + s(x)y(x, t) \quad (2)$$

- $m$ : Mass of the membrane
- $d(x)$ : Position dependent damping
- $s(x)$ : Position dependent stiffness

## Simplifying the equations

We introduce  $g(x, t)$  as follows:

$$g(x, t) = d(x)\dot{y}(x, t) + s(x)y(x, t) \quad (3)$$

Then rewrite  $m\ddot{y}(x, t)$  as:

$$m\ddot{y}(x, t) = p(x, t) - g(x, t) \quad (4)$$

This allows us to then rewrite Equation (1) as:

$$\frac{\partial^2 p}{\partial x^2}(x, t) - \kappa p(x, t) = -\kappa g(x, t) \quad (5)$$

Where  $\kappa = \frac{2\rho}{hm}$ .

## Simplifying the equations

Equation 5 can be further reduced to 2 first degree ODEs by introducing  $v$  as follows:

$$\frac{\partial y}{\partial t}(x, t) = v(x, t) \quad (6)$$

$$\frac{\partial v}{\partial t}(x, t) = \frac{p(x, t) - g(x, t)}{m} \quad (7)$$

Which can then be solved with a numerical integrator, say Classical Runge Kutta 4



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# Damping and Stiffness Terms

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$$d(x) = \epsilon\sqrt{m s(x)}$$

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$$d(x) = \epsilon\sqrt{m s(x)}$$

Non-linear damping term

$$d(x, \dot{y}) = \left\{ (1 - \gamma)(\delta_{sat} - \delta_{neg}) \left[ 1 - \frac{1}{1 + e^{(\Lambda - \alpha)/\mu_\alpha}} \right] + \gamma(\delta_{sat} - \delta_{neg}) \left[ 1 - \frac{1}{1 + e^{\Lambda - \beta/\mu_\beta}} \right] + \delta_{neg} \right\} \sqrt{m s(x)}$$

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$$s(x) = s_0 e^{-\lambda x}$$

# Damping and Stiffness Terms

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$$p(x, t) = m\ddot{y}(x, t) + d(x)\dot{y}(x, t) + s(x)y(x, t)$$

Linear stiffness term

$$s(x) = s_0 e^{-\lambda x}$$

Non-linear case; an additional delayed feedback stiffness term

$$c(x, \dot{y}) = \left\{ (1 - \gamma)(\sigma_{\text{zweig}}) \left[ \frac{1}{1 + e^{(\Lambda - \alpha)/\mu_\alpha}} \right] + \gamma(\sigma_{\text{zweig}}) \left[ \frac{1}{1 + e^{\Lambda - \beta/\mu_\beta}} \right] \right\} \quad (8)$$

# A Sample Model Output

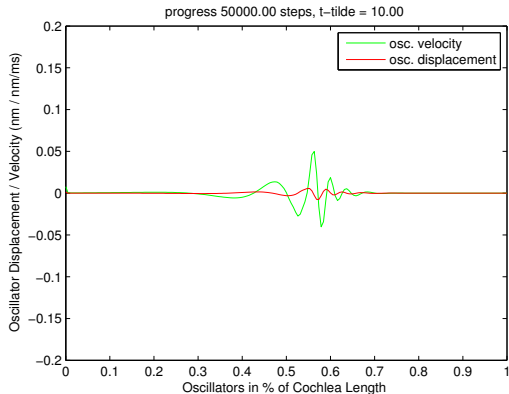


Figure: Modeling the response of the basilar membrane to a tone sound



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# Simulation Approach

- We have a good model of the normal cochlea
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- We have a good model of the normal cochlea
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## Idea

Find a method to get back the original sound from the model of a healthy ear. Use this method on a model of a damaged ear to simulate hearing loss

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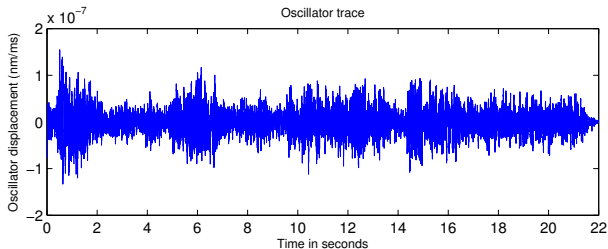
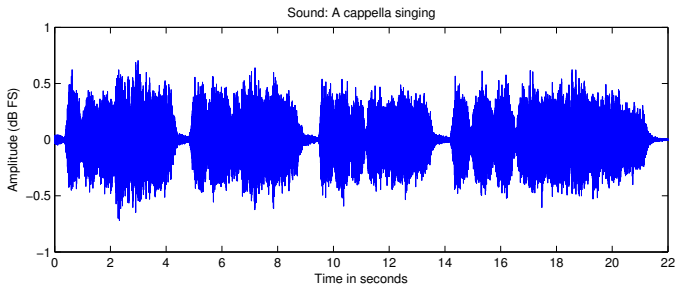
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# The Model Viewed as a Convolution



# Finding the Inverse Filter

If the original sound is  $x$  and the result from the model is  $y$  then the model is  $h$

$$y(t) = x(t) * h(t)$$

Performing a Fourier Transformation results in:

$$Y(f) = X(f) \cdot H(f)$$

A change in basic operation from convolution to multiplication

## Finding the Inverse Filter

Then  $H$  and  $H^{-1}$  are:

$$H(f) = \frac{Y(f)}{X(f)}$$
$$H^{-1}(f) = \frac{1}{H(f)}$$

$X(f)$  Can then easily be found

$$X(f) = \frac{Y(f)}{H(f)}$$

And then:

$$x(t) = \text{Inverse Fourier Transform of } (X(f))$$

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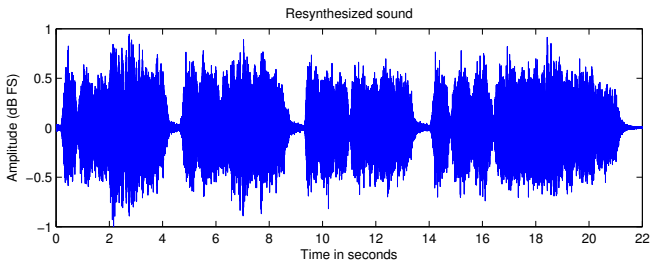
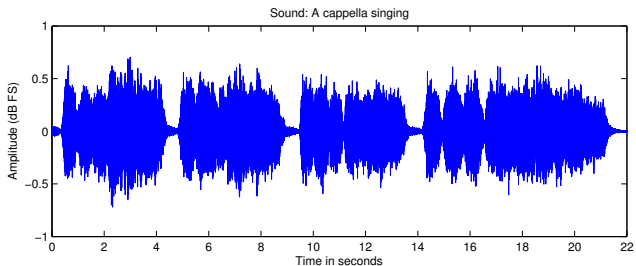
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# Some Results



# What Affects Sound Reproduction Quality

- Length of impulse response!!

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- Length of impulse response!!
- Type of window used, Gaussian seems to be a good choice
- Which oscillator is used
- Integration time step used (affects sound quality)
- Number of oscillators in the Model

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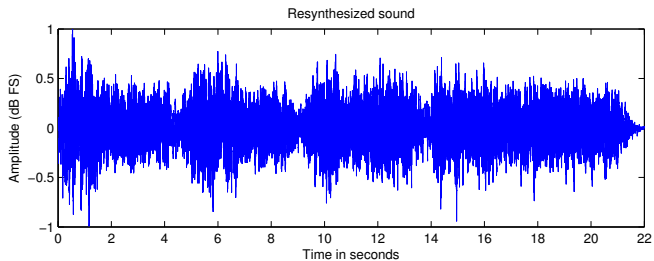
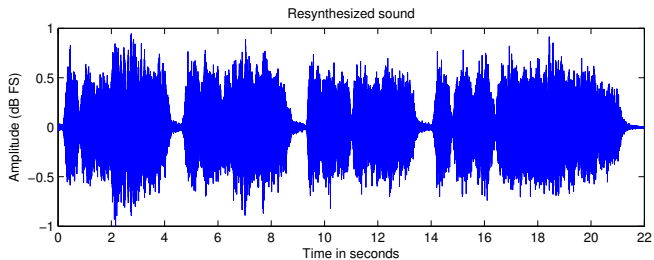
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# Testing

- Objective testing may be limited
- Subjective testing
  - Comparing two sounds on Right and Left channel does not work
  - Consecutive listening tends to work better
  - System limitations should be considered



# Testing and Optimization, a Possibility



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# Outlook

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# Outlook

- We have a good model of the ear
- Can we get good sound back from the model?
- Improving the sample rate
- Using multiple oscillators
- Look for optimality using the settings required for the Non-linear model
- Resynthesizing sound from the non-linear model